



Subject Name: Biomedical Instrumentation Design I_2

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Lecture No.: 3

Lecture Title: ECG PART 2.



- *Lead selector:*

- ✓ Determine which electrodes are necessary for a particular lead and to connect them to the remainder of the circuit

- *Preamplifier*

- ✓ Carries out the initial amplification of the ECG.
- ✓ Have very **high input impedance and a high CMRR**
- ✓ Three-op-amp **differential amplifier**

- *Isolation circuit*

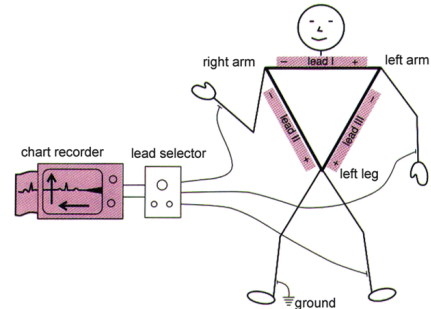
- ✓ To block dangerous currents (e.g. from 120V power line (50 or 60 Hz)) from flowing from the patient through the amplifier to the ground of the recorder or microcomputer.

- *Driven right leg circuit*

- ✓ provides a reference point on the patient that normally is at ground potential

- *Driver amplifier*

- ✓ Amplifies the ECG to a level at which it can appropriately record the signal.
- ✓ Its input is **AC-coupled** so that **offset voltages** amplified by the preamplifier are not seen at its input.
- ✓ carries out **bandpass filtering** of the ECG





Frequent Problems

To be considered in the design and application of the ECG machine and other biopotential amplifiers

- **Frequency Distortion**

- ✓ High-frequency loss rounds the sharp edges of the QRS complex.
- ✓ Low-frequency loss can distort the baseline (no longer horizontal) or cause monophasic waveforms to appear biphasic.

- **Saturation/cutoff Distortion**

- ✓ Combination of input signal amplitude & high offset voltage (at the electrodes) drives amplifier into saturation
- ✓ Positive case: clips off the top of the R wave
- ✓ Negative case: clips of the Q, S, P, and T waves

- **Ground Loops**

- ✓ Patients are connected to multiple pieces of equipment; each has a ground (power line or common room ground wire)
- ✓ If more than one instrument has a ground electrode connected to the patient, a ground loop exists. Power line ground can be different for each item of equipment (one higher than the other), sending current through the patient, elevating body potential, and introducing common-mode noise on ECG.
- ✓ Hospitals and clinics usually have established grounding systems for medical equipment.

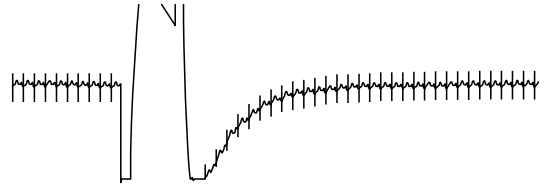
- **Open Lead Wires**

- ✓ Disconnected electrode to the machine, induce high potential in open wire
- ✓ Can be detected by impedance monitoring.



Artifacts

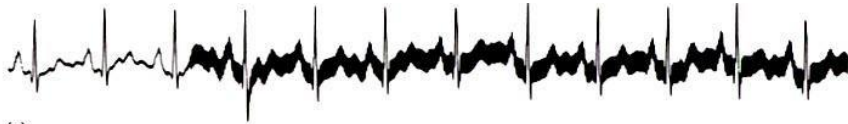
- Unwanted voltage transients
 - ✓ Electrical stimulation signals (high-voltage –current pulse), like defibrillation
 - ✓ Higher than ECG potentials
- Amplifier saturates, charge build-up on the coupling capacitor.
- Prolonged recovery to baseline
 - ✓ Recovery time set by the low-frequency corner of the bandpass amplifier
- Other sources
 - ✓ Motion of electrodes (body movement)
 - ✓ Static charges of patients
- Solution
 - ✓ Protection circuitry, discharge of patients, use of electrodes



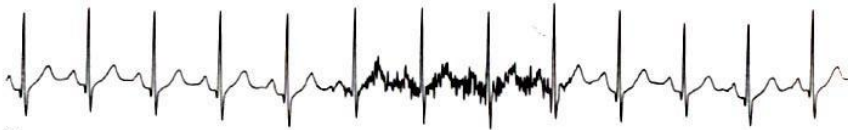
Effect of a voltage transient on an ECG recorded on an electrocardiograph in which the transient causes the amplifier to saturate, and a finite period of time is required for the charge to bleed off enough to bring the ECG back into the amplifier's active region of operation. This is followed by a first-order recovery of the system.



Artifacts: Interference from Electric Devices



(a)



(b)

- Upper figure: coupling of 60 Hz power line noise
 - ✓ **Electric-field coupling** between the power lines and the instrument, patient, and lead wires, like **small capacitors** joining these entities to the power lines
- Lower figure: coupling of electromyographic (EMG) noise
 - ✓ An example is tensing chest muscles while an ECG is being recorded.



Power-Line Coupling

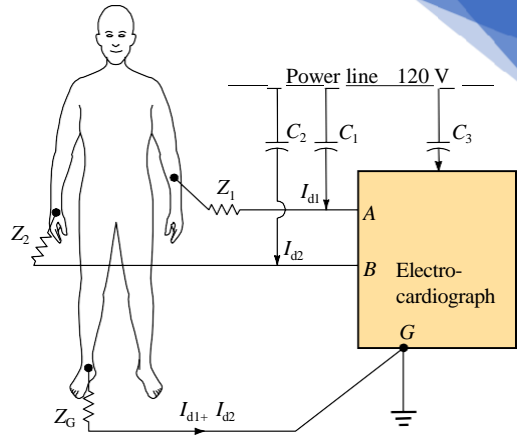
- Small parasitic capacitors (arise from the inherent electric field surrounding any charged conductor) **connect the power line to the RA and LA leads, and the grounded instrument case**
- Small ac displacement currents I_{d1} and I_{d2} are generated
- **The body impedance is about 500Ω and can be neglected**

$$v_A - v_B = i_{d1} Z_1 - i_{d2} Z_2 \quad (6.3)$$

- If I_{d1} and I_{d2} are approximately equal, and values measured for 9m cables show that $i_d = 6\text{nA}$, although this value will depend on the room and the location of other equipment and power lines. Skin-electrode impedances may differ by as much as $20 \text{ k}\Omega$. Hence:

$$\begin{aligned} v_A - v_B &= i_{d1} (Z_1 - Z_2) \quad (6.4) \\ &= (6 \text{ nA}) (20 \text{ k}\Omega) \\ &= 120 \mu\text{V} \end{aligned}$$

- Remedies
- Shield electrodes & connect to electrocardiograph (grounding tree) to reduce i_d
- Reduce or match the electrode skin impedances (minimize $Z_1 - Z_2$)

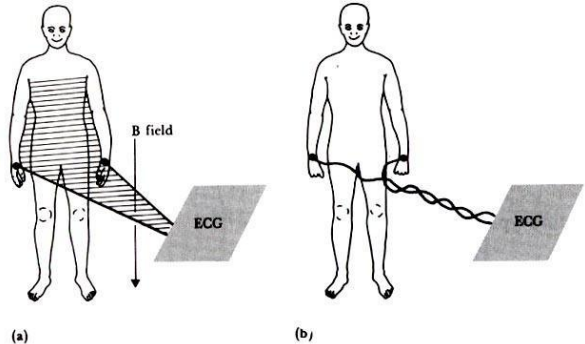


A mechanism of electric-field pickup of an electrocardiograph resulting from the power line. Coupling capacitance between the hot side of the power line and lead wires causes current to flow through skin-electrode impedances on its way to ground.



Magnetic Field Coupling

- Sources
- Power lines
- Transformers and ballasts in fluorescent lights
- Remedies
- Shielding
- Route leads away from potential sources
- Reduce the effective area of the single-turn coil (twist the lead wires)



Magnetic-field pickup by the electrocardiograph (a) Lead wires make a closed loop (shaded area) when patient and electrocardiograph are considered in the circuit. The change in magnetic field passing through this area induces a current in the loop.

(b) This effect can be minimized by twisting the lead wires together and keeping them close to the body in order to subtend a much smaller area.

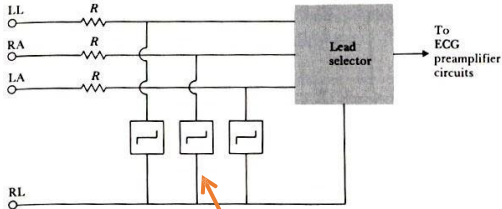


Other Sources of Interference

- Electromagnetic radiation
 - ✓ Patient leads become antennas, especially if detached.
- Sources
 - ✓ Radio
 - ✓ Television
 - ✓ Radar
 - ✓ High-freq generators
 - ✓ Research equipment
 - ✓ Electrosurgical devices
 - ✓ Arching fluorescent lights (needing replacement)
- Remedy
 - ✓ Employ capacitors shunting the inputs to the ECG amplifier to ground (eg., 200 pF).
 - ✓ Do not lower the input impedance of the amplifier.
- Other interferences: electrophysiological noise e.g. electromyographic (EMG) signal from muscle contraction, also picked up by ECG leads



Transient Protection

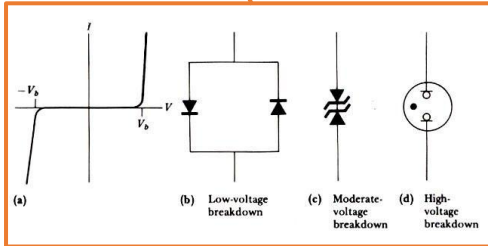


- High voltages due to electrosurgical equipment into patients and entering the ECG machine and cardiac monitor, causing damage and transient artifacts.
- Voltage limiting devices on each input lead are used to protect the equipment.

Figure 1 A voltage-protection scheme at the input of an electrocardiograph to protect the machine from high-voltage transients. Circuit elements connected across limb leads on left-hand side are voltage-limiting devices.

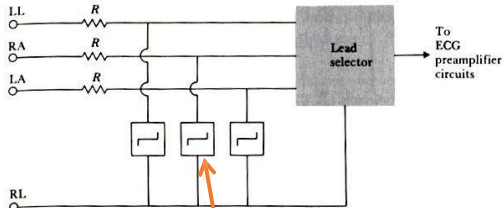
Figure 2 Voltage-limiting devices:

(a) *Current-voltage characteristics of a voltage-limiting device*, At voltages less than v_b , the breakdown voltage, the device allows very little current to flow and ideally appears as an open circuit. Once the voltage across the device attempts to exceed v_b , the characteristics of the device sharply change, and current passes through the device to such an extent that the voltage cannot exceed v_b as a result of the voltage drop across the series resistors R, and the device appears to behave as a short circuit in series with a constant-voltage source of magnitude v_b .





Transient Protection

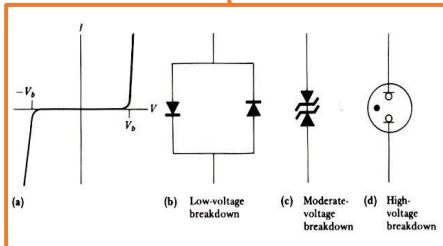


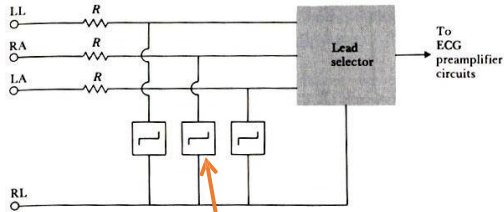
- High voltages due to electrosurgical equipment into patients and entering the ECG machine and cardiac monitor, causing damage and transient artifacts.
- Voltage limiting devices on each input lead are used to protect the equipment

Figure 3 A voltage-protection scheme at the input of an electrocardiograph to protect the machine from high-voltage transients. Circuit elements connected across limb leads on left-hand side are voltage-limiting devices.

Figure 4 Voltage-limiting devices

(b) *Parallel silicon-diode voltage-limiting circuit*, The diodes are connected such that the terminal voltage on one has a polarity opposite that on the other. The breakdown voltage is approximately 600 mV; thus, one of the diodes is forward-biased when the voltage reaches approximately 600 mV.





- High voltages due to electrosurgical equipment into patients and entering the ECG machine and cardiac monitor, causing damage and transient artifacts.
- Voltage limiting devices on each input lead are used to protect the equipment

Figure 5 A voltage-protection scheme at the input of an electrocardiograph to protect the machine from high-voltage transients. Circuit elements connected across limb leads on left-hand side are voltage-limiting devices.

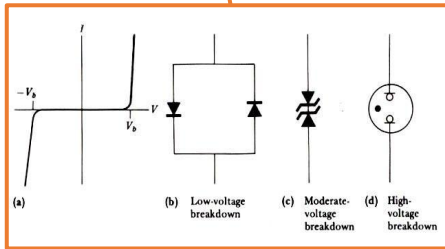
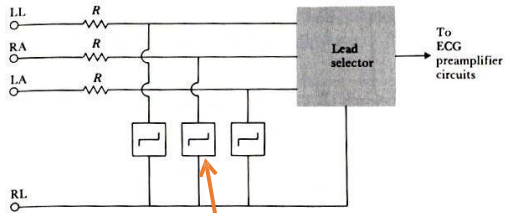


Figure 6 Voltage-limiting devices

(c) Back-to-back silicon Zener-diode voltage-limiting circuit.

When a voltage is connected across this circuit, one of the diodes is biased in the forward direction and the other in the reverse direction. The breakdown voltage in the forward direction is approximately 600 mV, but that in the reverse direction is much higher. It generally covers the range of 2 to 20 V. Thus, this circuit does not conduct until its terminal voltage exceeds the diode's reverse breakdown by approximately 600 mV.



- High voltages due to electrosurgical equipment into patients and entering the ECG machine and cardiac monitor, causing damage and transient artifacts.
- Voltage limiting devices on each input lead are used to protect the equipment

Figure 7 A voltage-protection scheme at the input of an electrocardiograph to protect the machine from high-voltage transients. Circuit elements connected across limb leads on left-hand side are voltage-limiting devices.

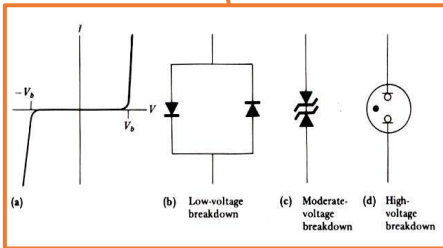


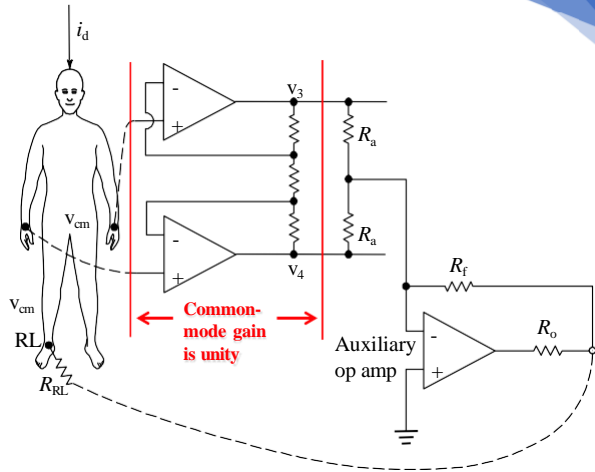
Figure 8 Voltage-limiting devices

- (a) Current–voltage characteristics of a voltage-limiting device,
- (b) Parallel silicon-diode voltage-limiting circuit,
- (c) Back-to-back silicon Zener-diode voltage-limiting circuit,
- (d) Gas-discharge tube (neon light) voltage-limiting circuit element.



Driven Right Leg Circuit

- Patient is not grounded
- Common mode voltage is sensed by two averaging resistors (R_a), inverted, amplified, and fed back to the right leg.
- Negative feedback drives the common mode voltage to a low value.
- Body's displacement current flows to the inverting OpAmp.
- *Provides safety*: if the OpAmp saturates, an alarm sounds; R_o limits current out of the feedback OpAmp.



Minimizes common-mode interference. The circuit derives common-mode voltage from a pair of averaging resistors connected to v_3 and v_4 in the instrumentation amp. The right leg is not grounded but is connected to output of the auxiliary op amp.